

1 **Tocopherol-loaded transfersomes: *in vitro* antioxidant activity and efficacy in skin regeneration**

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24 **ABSTRACT**

25 Transfersomes were prepared by using different polysorbates (i.e., Tween 20, 40, 60 and 80) and
26 loaded with tocopherol acetate, a naturally-occurring phenolic compound with antioxidant activity.
27 The vesicles showed unilamellar morphology, small size (~85 nm), low polydispersity index (≤ 0.27),
28 and high entrapment efficiency, which increased as a function of the length of the Tween fatty acid
29 chain (from 72% to 90%). The long-term stability of the formulations was evaluated by means of the
30 Turbiscan™ technology, which indicated their good stability, irrespective of the Tween used. The
31 vesicles efficiently delivered tocopherol to the skin, and showed biocompatibility *in vitro* in
32 keratinocytes and fibroblasts. Regardless of the Tween used, the transfersomes were able to protect
33 skin cells from the oxidative damage induced by hydrogen peroxide. Additionally, transfersomes
34 promoted cell proliferation and migration, which resulted in an acceleration of skin wound closure.
35 These results demonstrated that tocopherol-loaded transfersomes bear potential as topical delivery
36 system with antioxidant activity and wound healing properties.

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38 **Keywords:** Tocopherol; transfersomes; Tween; skin delivery; antioxidant activity; skin wound.

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40 **1. Introduction**

41 The use of naturally-occurring phenolic compounds to treat skin disorders has attracted considerable
42 interest in the last years. Phenolic compounds exhibit low toxicity and a series of biological activities,
43 including antioxidant, anti-inflammatory and antimicrobial activities with health-promoting effects.
44 Evidence suggests that phenols can alleviate symptoms and inhibit the development of various skin
45 disorders, such as skin aging, skin lesions, including wounds and burns, and even cancer development
46 (Działo et al., 2016). The wound healing efficacy of phenols has been attributed to their ability to
47 reduce the amount of reactive oxygen species (ROS) and inflammation developing in the wound, thus
48 promoting the induction of the skin repair mechanisms and accelerating the healing process
49 (Fitzmaurice et al., 2011).

50 Alpha-tocopherol represents the most abundant form of vitamin E, and is well-known for a strong
51 antioxidant activity, which resides on its ability to stabilize reactive species (Pegoraro et al., 2017).
52 Topically applied tocopherol has previously shown several beneficial and protective effects on the
53 skin. It is considered a photoprotector, as it can reduce ultraviolet (UV)-induced oxidative damage
54 (Lopez-Torres et al., 1998; McVean and Liebler, 1997). Tocopherol has also been shown to be able
55 to accelerate wound closure (Bonferoni et al., 2018; Horikoshi et al., 2018). Its role in repairing
56 injured skin is associated with its antioxidant activity, which counteracts the overproduction of ROS
57 involved in the pathogenesis of wounds (Schäfer and Werner, 2008). In addition, it has been
58 demonstrated that tocopherol accelerates wound repair by promoting cell polarization and migration
59 in human keratinocytes via phosphatidylinositol kinase/protein kinase C signalling cascade
60 (Horikoshi et al., 2018).

61 The administration of tocopherol is, however, limited by its poor water solubility and chemical
62 instability. The former can be increased by using tocopherol salts, and both can be improved by
63 incorporation in delivery systems (Pereira et al., 2015).

64 There are only a few scientific studies reporting on the effective incorporation of tocopherol in
65 nanocarriers. Tocopherol has been loaded in lipid nanoparticles, which provided effective protection
66 against UV-induced degradation, thus proving to be promising carriers for ensuring long-lasting
67 antioxidant benefits to the skin (Chen et al., 2017). In another study, tocopherol was loaded in
68 nanovesicles made of lecithin and hyaluronic acid, which were proposed as an innovative system for
69 the treatment of burn wounds (Pereira et al., 2016). Alternatively, chitosan oleate nanoemulsions
70 containing tocopherol were proposed as a wound healing system (Bonferoni et al., 2018). **Tocopherol**
71 **has been incorporated in phospholipid vesicles to improve its delivery to cells and tissues, while**
72 **acting as membrane stabilizing agent (Gonnet et al., 2010; Kagan, 1989). Moreover, it was found that**
73 **the incorporation of tocopherol in liposomes reduced lipid oxidation, which resulted in changes in**
74 **bilayer permeability (Hunt and Tsang, 1981).**

75 Given the poor literature on the topic, in the present study tocopherol in form of acetate salt was
76 loaded in transfersomes, ultradeformable vesicles first introduced in the early 1990s (Cevc and
77 Blume, 1992). Thanks to the elasticity generated by the incorporation of an edge activator in the lipid
78 bilayer structure, transfersomes have been shown to permeate through the stratum corneum lipid
79 lamellar regions as a result of their ability to squeeze through pores appreciably smaller than their
80 own size, and of the hydration or osmotic force in the skin (Cevc et al., 1998; Gupta et al., 2012).
81 Non-occlusive conditions are essential to generating a transepidermal osmotic gradient, which acts
82 as the driving force for elastic transport into the skin. Over the past years, transfersomes have been
83 used as carriers for a range of small molecules, peptides, proteins and vaccines, both *in vitro* and *in*
84 *vivo* (Cevc and Blume, 2001; Gupta et al., 2012; Jain et al., 2003).

85 In this study, tocopherol acetate loaded transfersomes were prepared with phosphatidylcholine and
86 different polysorbates (i.e., Tween 20, 40, 60 or 80), with the aim of investigating their feasibility for
87 non-invasive delivery to the skin, along with their antioxidant and wound healing potential. The
88 morphology, size, zeta potential and stability of the vesicles were evaluated, as well as their ability to

89 deliver tocopherol to the skin. The biocompatibility of the formulations was assessed *in vitro* in skin
90 cells, epidermal keratinocytes and dermal fibroblasts. Moreover, the ability of the formulations to
91 protect the cells from chemically-induced oxidative damage was studied, along with their ability to
92 stimulate cell proliferation and migration in order to achieve wound closure.

93 **2. Material and Methods**

94 **2.1. Materials**

95 Soy phosphatidylcholine (Lipoid S75) was purchased from Lipoid GmbH (Ludwigshafen, Germany).
96 Alpha-tocopherol acetate, Tween 20 (polyoxyethylene monolaurate), Tween 40 (polyoxyethylene
97 sorbitan monopalmitate), Tween 60 (polyoxyethylene sorbitan monostearate) and Tween 80
98 (polyoxyethylene sorbitan monooleate) were purchased from Galeno (Carmignano, Potenza, Italy).

99 **2.2. Vesicle preparation**

100 For the preparation of transfersomes, 180 mg of S75, 15 mg of Tween (20, 40, 60 or 80) and 15 mg
101 of tocopherol acetate were weighed in a glass vial and dispersed in 3 ml of water. After 4 hours, the
102 dispersions were sonicated with a high intensity ultrasonic disintegrator (20 cycles, 5 sec on and 2
103 sec off; 13 microns of probe amplitude). The vesicle dispersions (1 ml) were purified from the non-
104 incorporated tocopherol by dialysis against water (2 l) using Spectra/Por[®] membranes (12–14 kDa
105 MW cut-off, 3 nm pore size; Spectrum Laboratories Inc., DG Breda, the Netherlands) at room
106 temperature for 2 h **by replacing the water every 30 min. The water used (8 l total) was able to**
107 **theoretically remove the tocopherol contained in 1 ml of vesicle dispersion (5 mg).**

108 **2.3. Vesicle characterization**

109 Vesicle formation and morphology were evaluated by cryo-TEM analysis. A thin film of each sample
110 was formed on a holey carbon grid and vitrified by plunging (kept at 100% humidity and room
111 temperature) into ethane maintained at its melting point, using a Vitrobot (FEI Company, Eindhoven,
112 The Netherlands). The vitreous films were transferred to a Tecnai F20 TEM (FEI Company) and the

113 samples were observed in a low dose mode. Images were acquired at 200 kV at a temperature of
114 \sim -173 °C, using low-dose imaging conditions with a CCD Eagle camera (FEI Company).

115 The average diameter and polydispersity index (PI; a measure of the size distribution width) of the
116 vesicles were determined by dynamic light scattering using a Zetasizer nano-ZS (Malvern
117 Instruments, Worcestershire, UK). Zeta potential was estimated using the Zetasizer nano-ZS by
118 means of the M3-PALS (Mixed Mode Measurement-Phase Analysis Light Scattering) technique,
119 which measures the particle electrophoretic mobility. **For the mean diameter and zeta potential
120 analyses, samples (n=6) were diluted with water (1:100) and analysed at 25 °C.**

121 The entrapment efficiency (EE) of the transfersomes was calculated as the percentage of tocopherol
122 recovered after dialysis *vs.* the amount initially used. The content of tocopherol was determined by
123 high performance liquid chromatography (HPLC) after disruption of non-dialysed and dialysed
124 vesicles with methanol (1:100 dilution), using a Perkin Elmer Flexar chromatograph (Madrid, Spain).
125 The mobile phase was a mixture of methanol (97%) and ethanol (3%) delivered at a flow rate of 2
126 ml/min through a Brisa LC2 C₁₈ column (5 μ m, 15 \times 0.46 cm); detection was performed at 285 nm,
127 and a calibration curve was built by using standard solutions ($R^2 = 0.999$).

128 **2.4. Evaluation of vesicle stability**

129 The stability of the vesicles was evaluated by static multiple light scattering using the Turbiscan Lab
130 Expert (Formulation, l'Union, France) (Vitonyte et al., 2017). Samples (without dilution) were
131 placed in the test cell, and transmitted/backscattered light was monitored as a function of time (every
132 2 h) and cell height for 28 days at 30 °C using an Ageing Station (Formulation). The optical reading
133 head scanned the sample in the cell, providing Transmission (TS) and Backscattering (BS) data every
134 40 μ m in % relative to standards (suspension of monodisperse spheres and silicone oil), as a function
135 of sample height (in mm). The obtained profiles build up a macroscopic fingerprint of the sample at
136 a given time, providing useful information about changes in droplet size distribution, or appearance
137 of a creaming layer, or a clarification front with time.

138 **2.5. *In vitro* skin permeation studies**

139 Experiments were performed by using the dorsal skin of one day-old pigs (~1.5 kg) dead from natural
140 causes, provided by a local slaughterhouse. The skin was stored at $-20\text{ }^{\circ}\text{C}$ after excision, defrosted
141 and pre-equilibrated in saline (0.9% NaCl in water) 2 h before the experiments. The full-thickness
142 skin specimens ($n = 6$ per formulation) were sandwiched between the donor and receptor
143 compartments of Franz vertical cells with an effective diffusion area of 0.785 cm^2 . The receptor
144 compartment was filled with saline (~6.5 ml), thermostated at $37\pm 1\text{ }^{\circ}\text{C}$, and continuously stirred. The
145 transfersome dispersions were applied (100 μl) onto the skin surface, under non-occlusive conditions.
146 Every 2 h and up to 8 h, the receiving solution was withdrawn, refreshed and analysed by HPLC for
147 tocopherol content. After 8 h, the skin surface was gently washed with bidistilled water and blotted
148 on filter paper. The stratum corneum was removed by stripping with adhesive tape (Tesa[®] AG,
149 Hamburg, Germany). Epidermis was separated from dermis with a surgical scalpel. The tape strips
150 and the skin strata were cut, placed each in a flask with ethanol, and sonicated for 2 min in an ice bath
151 to extract the tocopherol. The tape and tissue suspensions were filtered out and assayed for tocopherol
152 content by HPLC.

153 **2.6. Cell viability assay**

154 Human keratinocytes (HaCaT) and mouse embryonic fibroblasts (3T3) (ATCC collection, Manassas,
155 VA, US) were grown as monolayers in 75-cm² flasks, incubated in 100% humidity and 5% CO₂ at
156 37 °C. Dulbecco's Modified Eagle Medium (DMEM) with high glucose, supplemented with 10%
157 foetal bovine serum, 1% penicillin/streptomycin, and 1% fungizone was used to culture both cell
158 lines. The cells were seeded into 96-well plates at a density of 7.5×10^3 cells/well, and after 24 h of
159 incubation were exposed for 48 h to tocopherol-loaded transfersomes properly diluted to yield
160 tocopherol concentrations of 20, 10, 1, and 0.1 $\mu\text{g/ml}$. Cell viability was assessed by adding MTT
161 [3(4,5-dimethylthiazolyl-2)-2,5-diphenyltetrazolium bromide] (100 μl , 0.5 mg/ml, final
162 concentration) to each well. After 3 h, the formazan crystals were dissolved in dimethyl sulfoxide,

163 and the absorbance was read at 570 nm. The experiment was repeated at least three times, each time
164 in triplicate. The results are presented as a percentage of untreated cells (100% viability).

165 **2.7. Protection against cellular oxidative stress**

166 HaCaT and 3T3 cells were seeded into 96-well plates and incubated at 37 °C for 24 h. The cells were
167 exposed to hydrogen peroxide (1:40000 dilution) and incubated for 4 h with the tocopherol-loaded
168 transfersomes at a final concentration of 1 µg tocopherol/ml. The cells were washed with phosphate-
169 buffered saline (PBS), and the viability was assessed by the MTT test. The measurement of cell
170 survival was used to quantify the protective effect of the formulations against hydrogen peroxide-
171 induced oxidative stress. Untreated cells were used as a negative control (100% viability), and cells
172 exposed to hydrogen peroxide-only were used as a positive control. The experiment was repeated at
173 least three times, each time in triplicate.

174 **2.8. *In vitro* scratch assay**

175 The ability of the tocopherol-loaded transfersomes to stimulate HaCaT and 3T3 proliferation and
176 migration was evaluated by measuring the cell expansion on wound surface (scratch assay). The cells
177 were seeded in 6-well plates until complete confluence was reached. Then, a linear scratch was
178 generated using a sterile plastic pipette tip. The scattered fragments of cells were removed by gently
179 washing with fresh medium. The cells were treated with the vesicular formulations (1 µg/ml
180 tocopherol) and incubated for 24 and 48 h. Untreated cells were used as a control. The speed of cell
181 migration and consequent wound closure was observed under a light microscope using a 10×
182 objective, thus assessing the efficacy of the formulations in wound healing.

183 **2.9. Statistical analysis of data**

184 Results are expressed as the mean±standard deviation. Analysis of variance (ANOVA) was used to
185 evaluate multiple comparison of means and Student's t-test was performed to substantiate differences
186 between groups using XLStatistics for Windows. The differences were considered statistically
187 significant for $p < 0.05$.

188 **3. RESULTS**

189 **3.1. Vesicle characterization**

190 Cryo-TEM micrographs showed that all the transfersomes were spherical, unilamellar and small in
191 size, below 100 nm (Figure 1), which points to the fact that the type of Tween used did not affect the
192 vesicle assembly. To complement these results, the mean diameter of the vesicles was measured by
193 dynamic light scattering, which provides a global estimation of the vesicle size calculated from the
194 scattering intensity of each particle population. As shown in Table 1, empty transfersomes were
195 around 85 nm in size, with good homogeneity ($PI \leq 0.27$) and highly negative zeta potential ($ZP \sim -63$
196 mV), due to the charge carried by S75. The encapsulation of tocopherol did not affect vesicle size,
197 while the zeta potential values were more negative (~ -80 mV; Table 1), due to the arrangement of
198 the phenol within the vesicles. It is noteworthy that the type of Tween used had a negligible effect on
199 the above parameters (i.e., size, PI, ZP), while it was a critical factor for the entrapment efficiency,
200 which was found to increase progressively as a function of the length of the Tween fatty acid chain
201 and the hydrophilic/lipophilic balance (HLB). The transfersomes containing Tween 20 (HLB 16.7)
202 had the lowest entrapment efficiency (72%), while the transfersomes containing Tween 80 (HLB 15)
203 had the highest entrapment efficiency (90%; Table 1).

204 The long-term stability of the transfersome formulations was evaluated by using the Turbiscan™
205 technology, which provides early information on possible destabilization processes occurring in a
206 colloidal dispersion, as it discriminates between reversible particle migration (sedimentation,
207 flocculation, or creaming), and irreversible particle-size change (coalescence). The Turbiscan™
208 measures the backscattering (BS) intensity versus sample height and aging time. This allows the
209 monitoring of particle diameter evolution and concentration change, as the BS is directly dependent
210 on the particle mean diameter and volume fraction. The main instability phenomena typically
211 observed in colloidal systems are particle migration (i.e., local variation of the concentration of
212 particles that causes a local variation of the BS level measured at the bottom and top of the sample)

213 and particle size increase (i.e., global variation of the particle size that causes a global variation of the
214 BS level measured in the middle of the sample).

215 As can be seen in the profiles depicted in Figure 2, all the transfersomes possessed good stability,
216 since BS variations ranged from 7% to 12%. Variations in size due to flocculation were observed in
217 the samples, and a peak appeared approximately after 10 days in the right part of the cell for
218 transfersomes containing Tween 20 and Tween 60, which indicates the occurrence of migration
219 phenomena to the upper part of the cell (creaming) caused by density differences between the vesicles
220 in dispersion and the continuous water phase.

221 These results point to the good stability of the prepared transfersomes, since even when instability
222 phenomena occurred, their reversibility (especially in the case of flocculation) allowed the re-
223 suspension of the vesicles by gentle shaking.

224 **3.2. *In vitro* skin permeation**

225 The skin delivery capabilities of transfersomes were evaluated under non-occlusive conditions, which
226 are crucial to generating a transepidermal osmotic gradient that drives the transport of the vesicles
227 and their payload into the skin. The accumulation of tocopherol in the main layers of the skin (i.e.,
228 stratum corneum, epidermis and dermis) and in the receptor compartment of the Franz cells, which
229 mimics the biological fluids, was quantified (Figure 3). The highest amounts were found in the
230 stratum corneum: approximately 8.5% for all the transfersomes, with the exception of the
231 transfersomes containing Tween 80, which provided a higher accumulation (>11%). The values of
232 accumulation in the epidermis and dermis were 3.5% and 5.5%, with no statistically significant
233 differences among the formulations. Overall, the accumulation of tocopherol in the whole skin was
234 around 18% as an average of the four formulations, with transfersomes containing Tween 80
235 providing the highest value (>19%).

236 The amount of permeated tocopherol was approximately 6.5%, regardless of the formulation applied
237 on the skin.

238 **3.3. *In vitro* biocompatibility and antioxidant activity**

239 The biocompatibility of tocopherol loaded transfersomes was evaluated by using both epidermal
240 keratinocytes (HaCaT) and dermal fibroblasts (3T3). No toxic effect was observed in HaCaT cells
241 exposed to the formulations, as the viability was unchanged compared with control untreated cells,
242 regardless of the tocopherol concentration tested (0.1-20 µg/ml; Figure 4), while a dose-dependent
243 decrease in viability (from ~95% to 75%; Figure 4) was observed in 3T3 cells. Since no statistically
244 significant differences were detected among the transfersomes ($p > 0.05$), it can be concluded that the
245 type of Tween used to prepare the transfersomes had no impact on the biocompatibility of the
246 formulations.

247 The antioxidant activity of the formulations was evaluated as a function of their ability to protect the
248 keratinocytes and fibroblasts from the damages induced by hydrogen peroxide as oxidative agent
249 (Figure 5). Both cell lines showed a ~65% viability when stressed with hydrogen peroxide, due to the
250 ROS produced in culture. When HaCaT cells were treated with the tocopherol-loaded transfersomes,
251 viability reached ~100%, thus highlighting the protective effect of the formulations against ROS
252 ($p < 0.05$ versus the cells treated with hydrogen peroxide only). The results from 3T3 cells treated with
253 the transfersomes disclosed an improved protection against the deleterious effects of hydrogen
254 peroxide, and a proliferative response (~115% viability on average) that was stronger when the
255 transfersomes containing Tween 40 were used (127% viability; $p < 0.05$).

256 **3.4. *In vitro* wound closure**

257 The ability of the formulations to promote both proliferation and migration of keratinocytes and
258 fibroblasts was assessed by the scratch assay, which involves the evaluation of cells spreading on the
259 wound area, consisting in a linear cut on the cell monolayer.

260 In HaCaT cells treated with transfersomes, a progressive decrease in the wound area was observed
261 with time, due to newly formed cells (Figure 6). After 24 h, the regeneration of the cell layer was
262 faster in the cells treated with transfersomes containing Tween 80, and the wound was almost

263 completely closed, as compared to untreated control cells. The cells treated with the other
264 transfersomes showed an intermediate rate of wound closure. After 48 h, the wound was still open in
265 untreated control cells, while it was closed in the cells treated with the transfersomes, with the
266 exception of those containing Tween 60.

267 In 3T3 cells, the transfersomes promoted wound closure, as compared to untreated control cells, in a
268 slower manner than in HaCaT cells (Figure 7). After 24 h, the scratch in untreated cells was basically
269 unchanged, while the wound area decreased in the cells treated with transfersomes, with an almost
270 complete closure when transfersomes containing Tween 80 were used. After 48 h of treatment with
271 the vesicular formulations, cell proliferation was stimulated leading to a significant reduction in
272 wound width when transfersomes containing Tween 20, 40 and 60 were used, and a complete closure
273 when the transfersomes containing Tween 80 were used. These results point to a key contribution of
274 the formulations in improving cell proliferation and migration at the wound site, and wound healing.

275 **4. Discussion**

276 Our objective in this study was to suppress the increased levels of ROS associated with wounds that
277 damage the cells, by localized delivery of antioxidant tocopherol, and stimulate skin regeneration at
278 the wound site. To achieve this objective, tocopherol-loaded transfersomes were developed to carry
279 and deliver the phenol to the skin. The transfersome formulation was optimized using different
280 polysorbates (i.e., Tween 20, 40, 60, and 80), which weakly affected the physico-chemical features
281 of the vesicles (i.e., size, morphology, stability) and their technological (entrapment efficiency and
282 transdermal diffusion) and physiologically relevant properties required for wound healing (e.g.,
283 antioxidant and regenerative properties). The results showed that the transfersomes were small in size
284 (<100 nm), with high entrapment efficiency (up to 90%), and stable on storage. The elastic vesicles
285 provided a good distribution of tocopherol in the skin strata, as well as its permeation into the systemic
286 circulation. Additionally, the biocompatibility of the formulations, their protective effect against
287 oxidative damage, and their wound healing potential were demonstrated *in vitro* in keratinocytes and

288 fibroblasts. These skin cells have a relevant role in wound healing, and their proliferation is essential
289 for the complete restoration of the epithelium damaged during lesions (Bainbridge, 2013; Mansbridge
290 and Knapp, 1987). The tocopherol-loaded transfersomes applied at the wound site were able to inhibit
291 the tissue damage caused by the free radicals generated during injury thanks to the antioxidant activity
292 of tocopherol, stimulate the proliferation and migration of skin cells, and accelerate the wound healing
293 process, as demonstrated by the assessment of the speed and degree of wound closure. Previous
294 studies have demonstrated the beneficial effects in wound healing of raw tocopherol when given
295 orally (Musalmah et al., 2005), or of a tocopherol cream applied topically in diabetic rats (Lin et al.,
296 2012), or of tocopherol in chitosan oleate nanoemulsions tested *in vitro* in keratinocyte and fibroblast
297 cell cultures and *ex vivo* in skin biopsies (Bonferoni et al., 2018). To the best of our knowledge, this
298 is the first study reporting on the potential acceleration of wound healing by topical delivery of
299 tocopherol via transfersomes, especially transfersomes containing Tween 80.

310 **5. Conclusion**

311 The study suggested the successful development of vesicular formulations that could be used to help
312 control wound oxidative stress, and thereby accelerate wound healing. The type of polysorbate used
313 to prepare the tocopherol loaded transfersomes weakly affected the properties and performances of
314 the vesicles, but the transfersomes containing Tween 80 can be regarded as the most promising
315 formulation, as the vesicles were small (76 nm) and capable of incorporating the highest amount of
316 tocopherol (90%). In addition, they were able to improve, to a better extent, the deposition of
317 tocopherol in the different skin strata, and to ensure the complete closure of the wound. Additional
318 investigations, such as targeted *in vivo* tests, are needed to validate the *in vitro* antioxidant and wound
319 healing activities of the prepared tocopherol loaded transfersomes.

320

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401 **Figure captions**

402 **Figure 1.** Cryo-TEM images of tocopherol transfersomes prepared with Tween 20, 40, 60 or 80: A,
403 T20Transfersomes; B, T40Transfersomes; C, T60Transfersomes; D, T80Transfersomes.

404 **Figure 2.** Stability study of the transfersomes performed by using the Turbiscan® technology.
405 Backscattering profiles of transfersomes containing Tween 20, 40, 60 or 80 over 28 days at 30 °C. A,
406 T20Transfersomes; B, T40Transfersomes; C, T60Transfersomes; D, T80Transfersomes.

407 **Figure 3.** *In vitro* skin permeation studies: amount of tocopherol accumulated in the skin layers (SC,
408 stratum corneum; Ep, epidermis; D, dermis) and receptor fluid (RF) after 8 h of non-occlusive
409 application of the transfersomes. Each value is the mean \pm standard deviation of six experimental
410 determinations.

411 **Figure 4.** Viability of keratinocytes (HaCaT) and fibroblasts (3T3) incubated for 48 h with tocopherol
412 transfersomes. Data are reported as mean values \pm standard deviations of cell viability expressed as
413 the percentage of control (untreated cells; 100% of viability).

414 **Figure 5.** Antioxidant protective effect of tocopherol transfersomes against hydrogen peroxide-
415 induced oxidative stress in keratinocytes (HaCaT) and fibroblasts (3T3). Data are reported as mean
416 values \pm standard deviations of cell viability expressed as the percentage of control (untreated cells;
417 100% of viability).

418 **Figure 6.** Optical microscopy images of wound closure in keratinocytes (HaCaT) as a function of the
419 treatment with transfersomes for 0, 24 and 48 h, in comparison with untreated control cells. Bars
420 correspond to 500 μ m.

421 **Figure 7.** Optical microscopy images of wound closure in fibroblasts (3T3) as a function of the
422 treatment with transfersomes for 0, 24 and 48 h, in comparison with untreated control cells. Bars
423 correspond to 500 μ m.

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