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**This is the Author's [*accepted*] manuscript version of the following contribution: Cau R, Bassareo PP, Porcu M, Mannelli L, Cherchi V, Suri JS, Saba L. Pulmonary transit time as a marker of diastolic dysfunction in Takotsubo syndrome. Clin Radiol. 2023 Nov;78(11):e823-e830.**

**The publisher's version is available at:  
10.1016/j.crad.2023.06.013**

**When citing, please refer to the published version.**

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1 **Pulmonary transit time as a marker of diastolic dysfunction in**  
2 **Takotsubo syndrome.**

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**Keywords:** Takotsubo; CMR; Pulmonary transit time; diastole; first-pass

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50 **Key points**

- 51       • PTT was suggested as a feasible CMR tool to assess diastolic dysfunction.
- 52       • TS patients showed higher PTT, PTTI, and PBVI values in comparison with healthy
- 53       controls.
- 54       • PTT and its derived parameters may be new tools in evaluating the diastolic function in TS
- 55       patients.

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57

58 **Abbreviations**

59 **TS** Takotsubo syndrome

60 **LV** left ventricle

61 **RV** right ventricle

62 **CMR** cardiac magnetic resonance

63 **TTE** transthoracic echocardiography

64 **PTT** Pulmonary transit time

65 **PTTI** Pulmonary transit time index

66 **PBVI** Pulmonary blood volume index

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72 **Introduction**

73 Takotsubo syndrome (TS) is a well-recognized form of cardiomyopathy characterized by a  
74 specific pattern of left ventricular (LV) dysfunction, presenting as apical ballooning and hyperkinesis  
75 of basal segments the most<sup>ly</sup>. Less common variants of the disease can involve mid-ventricular, basal,  
76 and focal LV segments or the whole LV or both ventricles, or just the right ventricle (RV)<sup>1-4</sup>. Along  
77 with LV systolic impairment, diastolic dysfunction can arise in a significant number of TS patients  
78 during the transient course of the cardiomyopathy<sup>5-7</sup>. Not only, but the onset of diastolic dysfunction  
79 is known to have a prognostic negative impact on TS clinical outcome<sup>6</sup>.

80 Pulmonary transit time (PTT) is a previously studied tool to evaluate cardiopulmonary  
81 function and provide information regarding an increase in LV filling pressure, a condition which has  
82 been termed diastolic dysfunction or “hemodynamic congestion”<sup>8</sup>. PPT can be measured either  
83 invasively, by using cardiac catheterization, or by means of non-invasive modalities, such as  
84 radionuclide imaging, computed tomography, echocardiography, and cardiac magnetic resonance  
85 imaging (CMR)<sup>9</sup>. Several recent studies have investigated the role of PTT using CMR<sup>8,10-12</sup> and noted  
86 prolonged PTT and derived parameters in patients with heart failure<sup>6</sup>. On the other hand, CMR is  
87 used in daily practice to evaluate TS<sup>13</sup>

88 The aim of this study was to evaluate PTT and its linked parameters in patients with TS as a  
89 marker of diastolic dysfunction and its association with echocardiography and CMR parameters.

90

## 91 **Material and Method**

### 92 *Study population*

93 In this retrospective single-center study, we searched in our database all the patients who  
94 underwent CMR between March 3<sup>rd</sup>, 2017, and February 7<sup>th</sup>, 2021, because of clinical suspicion of  
95 apical ballooning TS. We enrolled only TS patients with LV diastolic dysfunction assessed by  
96 Doppler echocardiography, as described previously<sup>14</sup>

97 A total of 42 subjects were finally included in the study cohort. Of those, 22 were TS and 20  
98 were controls.

99 TS diagnosis was made using the current definition as reported in the Position Statement of the  
100 European Society of Cardiology Heart Failure Association<sup>15</sup>. The diagnostic criteria include regional  
101 wall motion abnormalities not limited to a single epicardial vascular distribution region, which are  
102 usually preceded by a stressful trigger, in the absence of culprit atherosclerotic disease as assessed by  
103 invasive catheterization; new ECG abnormalities; elevated serum natriuretic peptide and a small  
104 increase in cardiac troponin; and recovery of LV dysfunction at follow-up.

105 Exclusion criteria included: subjects < 18 years; contraindication to CMR (such as implantable  
106 devices, severe claustrophobia), or history of significant renal disease with a eGFR < 30 mL/min/1.73  
107 m<sup>2</sup>; and coronary artery disease.

108 Controls were age-, sex- matched and underwent CMR to rule out scar-related ventricular  
109 tachycardia. Controls were included if CMR showed no signs of structural heart defects. The  
110 Institutional Review Board approval for this retrospective, cross-sectional study was obtained, and  
111 patient's consent was waived because of the retrospective nature.

112 A flowchart demonstrating the application of inclusion and exclusion criteria is provided in  
113 **Figure 1.**

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#### 117 *CMR acquisition*

118 All CMR scans were performed at 4.1±2.6 days (median = 1 day, range = 1-10 days) after  
119 admission to the hospital by using a Philips Achieva Stream 1.5 T scanner system (*Philips*  
120 *Healthcare, Best, The Netherlands*). Anterior coil arrays were used. Cine-CMR examinations were  
121 electrocardiogram triggered and performed during breath-holding. Thirty phases were derived for  
122 each cardiac cycle. The CMR protocol was based on functional sequences, such as cine white blood

123 steady-state free precession (SSFP) on the short and long axes (2 chambers, 3 chambers, and 4  
124 chambers). CMR perfusion was performed with the first-pass perfusion technique, with a bolus of  
125 contrast media injection (Gadovist, Bayer Healthcare, Berlin, Germany) with a dose of 0.15 ml per  
126 kg body weight. Image acquisition was begun at the same time as the contrast media injection using  
127 a cardiac-gated saturation-recovery sequence. Perfusion imaging was acquired in three short-axis  
128 views (basal, middle, and apical). LGE imaging was performed 10-12 minutes after contrast media  
129 injection (Gadovist, Bayer Healthcare, Berlin, Germany) with a dose of 0.15 ml per kg body weight  
130 using phase-sensitive inversion recovery sequences acquired in both short and long axis. The correct  
131 inversion time was determined using the Look-Locker technique.

132

### 133 *CMR image post-processing*

134 The commercially available software system Circle CVI42 (CVI42, Circle Cardiovascular  
135 Imaging Inc., Calgary, Canada) was used for PTT and its related parameters analysis. First-pass  
136 images were obtained with a bolus of gadolinium-contrast agent, thus allowing to evaluate an image  
137 for each heartbeat. PTT represents the number of cardiac cycles required for a bolus to pass from the  
138 RV to the LV. Briefly, a region of interest (ROI) was placed in the basal slice of RV and automatically  
139 copied in the entire stack of images, with manual correction when required. The second region of  
140 interest was positioned in the basal slice of LV. The average signal intensity and a signal intensity/  
141 time curve was obtained for both ROIs in every image. PTT was measured as the peak-to-peak time  
142 between the two curves. Conversely, pulmonary transit time index (PTTI) represents the PTT values  
143 corrected for heart rate, according to Bazett's Formula:

$$144 \quad \mathbf{PPTI (s)/\sqrt{R-R interval (s)}}$$

145 Finally, PBVI was calculated as the product of RV stroke volume index (RVSVI) and PTTI (**Figure**  
146 **2**):

$$147 \quad \mathbf{PBVI (ml/m^2) = RVSVI \times PPTI}$$

148 CMR feature tracking analyses of atrial deformation was conducted offline. Left atrial (LA) and right  
149 atrial endocardial borders were manually traced on long axis view of the cine images when the atrium  
150 was at its minimum volume. In particular, the four-, three-, and two-chamber views were used to  
151 derive LA longitudinal strain. LA appendage and pulmonary veins were excluded from segmentation.  
152 The right atrial longitudinal strain was based on the four-chamber view only. After manual  
153 segmentation, the software automatically tracked the myocardial borders throughout the entire  
154 cardiac cycle. The quality of the tracking and contouring was visually validated and manually  
155 corrected by a radiologist with 3 years of experience in cardiac imaging. There are three peaks in the  
156 strain curve, including reservoir, conduit, and booster strain. Accordingly, their corresponding strain  
157 rate parameters were included. **Figure 3.**

158 Global and regional T2 mapping were assessed on the same commercial post-processing software  
159 (*CVI42, Circle Cardiovascular Imaging Inc., Calgary, Canada*) by manually tracing endocardial and  
160 epicardial contours. A 10% safety margin was automatically set for both borders to prevent  
161 contamination from the blood pool and neighboring tissues. Finally, the reference point was set at the  
162 right ventricle insertion to generate a 16-segment AHA model.

163

#### 164 *Transthoracic echocardiography*

165 All patients underwent transthoracic echocardiography (TTE) before the CMR examination  
166 (the median time interval was 3 days, ranging from 1 to 8 days). TTE allowed assessing LV diastolic  
167 function in terms of traditional and Tissue Doppler-derived parameters, such as mitral valve E/A,  
168 deceleration time of E wave, E/e'. TTE was carried out in agreement with the current international  
169 guidelines <sup>14</sup>.

170

#### 171 *Statistical analysis*

172 Continuous variables are presented as mean  $\pm$  standard deviation (SD). Kolmogorov-Smirnov  
173 tests were used to check continuous variables for normal distribution. Comparisons of continuous

174 data were performed using independent samples t test or Mann-Whitney U test analysis. Categorical  
175 variables were compared using chi-square or Fisher's exact test, according to the data distribution.  
176 A receiver-operating characteristic (ROC) analysis was performed to calculate optimal thresholds and  
177 areas under the curves (AUCs). The Youden index was used to depict optimal cut-off values from the  
178 ROC curves. Sensitivities and specificities were calculated for these cut-off values with 95%  
179 confidence intervals. Correlation was assessed using the Pearson r and Spearman rho coefficient  
180 according to data distribution. Binary logistic regression was used to assess the value of PTT  
181 parameters for identification of TTC patients. PTT values were incorporated into univariable analysis  
182 as continuous variables, and age, gender, and CMR significant parameters ( $P < 0.05$ ) were then  
183 included into multivariable analysis.

184 A p-value  $< 0.05$  was considered statistically significant. All statistical analysis was performed  
185 using IBM SPSS Statistics version 22 (SPSS Inc., Chicago, IL, USA).

186

## 187 **Results**

188 *Patient demographics, clinical and echocardiography data.*

189 Twenty-two TS patients (20 females, mean age  $68,9 \pm 9,2$  years.), and 20 healthy subjects (17  
190 females, mean age  $67,3 \pm 10,2$  years) were identified. Comparison of patient's baseline  
191 characteristics, echocardiography, CMR, and PTT with its derived parameters between control and  
192 patients are summarized in **Table 1**.

193

194 *Pulmonary transit time in TS patients*

195 PTT and its derived parameters are reported in **Table 1**. PTT, PTTI, and PBVI were significantly  
196 higher in TS patients in comparison with the control group ( $p= 0.0001$ ,  $p=0.0001$ , and  $p=0.002$ ,  
197 respectively) (**Figure 4**). PTT (OR 0.38; 95% CI 0.20-0.72,  $p=0.003$ ), PTTI (OR 0.41; 95% CI 0.22  
198 -0.74,  $p=0.003$ ), and PBVI (OR 0.98; 95% CI 0.96 - 0.99,  $p=0.009$ ) were significantly associated with



199 the presence of TTC in univariable analysis. Using multivariable logistic regression analysis, PBVI  
200 was the only independent discriminator between TTC and ACS (OR 1.01; 95% CI 0.97-1.21, p=0.03;  
201 **Table 2**)

202

203

204 *PTT in relation to echocardiography and CMR data.*

205 PBVI was significantly associated with a well-established TTE index of diastolic dysfunction,  
206 in particular E/e' ratio, E/A, and E wave deceleration time at Tissue Doppler (r= 0.643, p =0.001; r=  
207 0,443 p= 0,021 and r= 0,719 p= 0,001, respectively). **Figure 5** showed the relationship between  
208 pulmonary blood volume (PBVI) and echocardiography indices of diastolic dysfunction. In addition,  
209 PBVI demonstrated a significant correlation with global T2 mapping (r= 0,520, p=0,019).

210 The left atrial size was a mean of 13,2 cm<sup>2</sup>/m<sup>2</sup> and showed no correlation with PBVI (r=0,220,  
211 p=0,310). Conversely, left atrial strain and strain rate parameters correlated significantly with PBVI  
212 (**Table 3**). There was no other statistically significant correlation between PTT and CMR parameters.

213

214 *ROC analysis*

215 PTT, PTTI, and PBVI proved to have good-to-excellent sensitivity in differentiating patients  
216 with TS from healthy controls (AUCs of 0.90, 0.91, and 0.84, respectively). For PBVI the optimal  
217 cut-off value to identify TS was > 332.76 with a sensitivity and specificity of 70% and 90%  
218 respectively. (**Figure 6**)

219

## 220 **Discussion**

221 This study was carried out to non-invasively assess with new CMR parameters the diastolic  
222 function in TS patients and give an insight into the pathophysiology of the disease. PTT has been  
223 widely recognized as an important tool capable of providing useful information regarding the  
224 presence and severity of diastolic dysfunction during other cardiac diseases<sup>8-11</sup>.

225 The main findings can be summarized as follow: (1) TS patients have longer PTT/PTTI and  
226 higher PBVI values in comparison with controls; (2) PBVI is related to diastolic dysfunction at TTE;  
227 (3) PTT and its related parameters have good-to-excellent diagnostic accuracy in detecting a diastolic  
228 impairment in TS.

229 A prompt and non-invasive assessment and grading of LV congestion is highly desirable in  
230 clinical practice. This is primarily because a non-invasive evaluation has the potential to detect LV  
231 congestion before it become clinically evident<sup>16</sup>. Currently, invasive cardiac catheterization is  
232 considered the gold standard to measure intracardiac filling pressure, but it is not without any risk for  
233 the patient. For these reasons, several non-invasive methods have been proposed. Among them,  
234 echocardiography represents the reference standard in the evaluation of LV diastolic function<sup>14</sup> but,  
235 at the same time, its diagnostic value is limited in case of poor acoustic windows, such as in  
236 overweight/obese subjects or patients with respiratory diseases<sup>17-19</sup>.

237 On the other hand, CMR is the reference technique in the non-invasive assessment of cardiac  
238 systolic function and volumes. It allows tissue characterization as well, unlike TTE<sup>3,20,21</sup>. In the setting  
239 of TS, CMR enables detection of typical regional wall motion abnormalities as well as the possible  
240 reversible and irreversible myocardial damage at late gadolinium enhancement, thus providing a  
241 precise characterization of TS<sup>3</sup>.

242 Although the role of CMR in evaluating ventricular diastolic function has not been fully  
243 elucidated yet, it has been suggested that it may play a role in this scenario as well. Recently, Ricci  
244 et al proposed PBVI as a quantitative marker to detect and quantify diastolic dysfunction in heart  
245 failure due to different etiologies<sup>8,10</sup>.

246 TS is an acute ventricular dysfunction characterized by a diverse spectrum of outcomes, ranging from  
247 favorable to life-threatening<sup>22</sup>. While it is well known that TS is characterized by a transient form of  
248 ventricular systolic dysfunction with different patterns, the most frequent of which is apical  
249 ballooning along with hyperkinesis of basal segments, several studies suggested a possible  
250 concomitant diastolic involvement<sup>7</sup>. In the setting of TS, diastolic dysfunction is generally considered

251 to occur in close temporal correlation with segmental wall motion abnormalities<sup>23</sup>. Ahtarovsky et al.  
252 reported that despite a rapid restoration of systolic function, there was a delayed recovery of diastolic  
253 function, suggesting that LV relaxation may be compromised for an extended period<sup>7</sup>. Similar results  
254 were obtained by Medeiros et al., who demonstrated LV inability to fill adequately at normal pressure  
255 due to myocardial stiffness<sup>5</sup>. Again, Sun et al. described an abnormal diastolic function in 53 % of  
256 the 205 enrolled TS patients. At multivariate analysis, both persistent diastolic and systolic  
257 dysfunction were independent predictors of a poor outcome<sup>6</sup>. The trigger of diastolic dysfunction is  
258 usually represented by an increase in LV stiffness with consequent inability to properly relax, which  
259 in turn increases LV filling pressure and left atrial contractility<sup>4,24-28</sup>. Consequently, it was not  
260 surprising a significant correlation was found between PBVI and atrial strain parameters.

261 Fibrosis may be the underlying cause of LV dysfunction in TS<sup>29</sup>. In this respect, an  
262 immunohistological study showed an increase in collagen-1 subfraction content in the myocardial  
263 areas with late gadolinium enhancement<sup>30</sup>. Our study demonstrated a significant correlation between  
264 PBVI and T2 mapping. It is well known that myocardial edema impairs myocyte function and is  
265 responsible for diastolic impairment with decreased LV chamber compliance<sup>31,32</sup>. Based on this  
266 finding, we can speculate on another theory that sees myocardial edema as one of the determining  
267 factors of diastolic impairment in TTC patients.

268 Nevertheless, further studies are needed to clarify the role of myocardial edema fat in the  
269 course of diastolic dysfunction in TTC.

270 PTT/PTTI and PBVI already showed their ability as markers of diastolic dysfunction in  
271 different cardiac insufficiency scenarios and correlated with many clinical parameters<sup>6,8</sup>. The results  
272 of this study suggest that PTT and its derived parameters may be useful CMR-related tools for  
273 diastolic dysfunction in TS patients and may be used to refine the diagnosis of the disease. To our  
274 knowledge, this is the first study examining these parameters in the TS setting.

275 A major limitation of this research is certainly the relatively small sample size and the  
276 retrospective selection of the patients. However, all patients were very homogeneous, as we enrolled

277 only subjects with the classic apical ballooning subtype. The promising results of the study need to  
278 be confirmed with larger cohorts of patients. Moreover, the predictive value of PTT in terms of  
279 adverse cardiovascular events has not been assessed.

280 Finally, the hemodynamic congestion **parameters derived by CMR** in TS patients would have  
281 been probably different if CMR had been performed within a shorter period **compared to**  
282 **echocardiography**, ideally on the same day of hospital admission.

283

284

## 285 **Conclusion**

286 In this study, TS patients showed significantly higher PTT and derived parameters values in  
287 comparison with control group owing to the onset of diastolic dysfunction. PTT and PBVI may be  
288 additional CMR tools in refining TS pathophysiology.

289

290

## 291 **Disclosure**

292 All authors agreed with the content and gave consent to submit.

293 All authors contributed equally as authors to this work.

294 The authors state that this work is not under consideration elsewhere and none of the paper's  
295 contents have been previously published.

296 This research did not receive any specific grant from funding agencies in the public, commercial, or  
297 not-for-profit sectors.

298 All authors read and approved the final manuscript.

299 The scientific guarantor of this publication is the corresponding author.

300 The authors declare that they have no competing interests.

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## 418 **Figure legends**

419 **Figure 1** A flowchart demonstrating the application of inclusion and exclusion criteria.

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421 **Figure 2** An example of pulmonary transit time analysis (PPT) in Takotsubo (a) and control group  
422 (b). As reported in the Method section, PPT was measured as the peak-to-peak time between the two-  
423 signal intensity/time curves, obtained with a ROI in the left and right ventricle, respectively.

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425 **Figure 3:** Representative image of the different phases of left atrial strain, including reservoir, conduit  
426 and booster phase from 2-chambers view using CMR in a TS patient.

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428 **Figure 4** Box-Whisker plots representing the difference in PPT, PPTI and PBVI between Takotsubo  
 429 patients and controls.

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431 **Figure 5** Correlation analysis showed the relationship between pulmonary blood volume (PBVI) and  
 432 echocardiography indices of diastolic dysfunction, in particular  $E^I/e^I$ , E/A and E wave deceleration  
 433 time.

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435 **Figure 6** ROC Curves for PPT, PPTI, and PBVI to identify the patients with Takotsubo.

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440 **Tables**

<b>Table 1: Comparison of Demographic features, TTE and CMR characteristics.</b>			
	TS	Control	p
Age (years)	68,95 ± 9,2	67,33 ± 20,22	0,54
Gender (females)	20/22 (91%)	17/20 (85%)	0,32
Heart rate (bpm)	70,14 ± 11	66,7 ± 7,9	0,46
BSA (m <sup>2</sup> )	1,65 ± 0,15	1,79 ± 0,23	0,095
EDV/BSA LV (mL/m <sup>2</sup> )	73,9 ± 15,33	82,82 ± 16,6	0,15
ESV/BSA LV (mL/m <sup>2</sup> )	30,68 ± 9,83	32,29 ± 8,27	0,56
SV/BSA LV (mL/m <sup>2</sup> )	42,88 ± 10,36	50,29 ± 10,38	0,69
LVEF (%)	54,7 ± 8,33	61,2 ± 4,6	0,36

EDV/BSA RV (mL/m <sup>2</sup> )	57,1 ± 12,43	75,8 ± 19,6	0,57
ESV/BSA RV (mL/m <sup>2</sup> )	23,4 ± 6	33,9 ± 9,7	<b>0,039</b>
SV/BSA RV (mL/m <sup>2</sup> )	35,3 ± 7,3	42,2 ± 11,3	0,068
RVEF (%)	59,4 ± 5,8	55,6 ± 2,9	0,58
E/A	0,90 ± 0,37	1,25 ± 0,43	<b>0,019</b>
E wave (cm/s)	237,66 ± 69,55	229,5 ± 56,52	0,91
E/e	15,67 ± 14,67	8,45 ± 2,33	<b>0,013</b>
PPT (s)	8,75 ± 2,22	5,16 ± 1,46	<b>0,0001</b>
PPTI (s)	10,1 ± 3,2	5,74 ± 1,77	<b>0,0001</b>
PBVI (ml/m <sup>2</sup> )	404,34 ± 107,03	255,72 ± 70,84	<b>0,002</b>
Left atrial area (cm <sup>2</sup> /m <sup>2</sup> )	13,2 ± 1,3	12,8 ± 1,1	0,59
Reservoir	24,66 ± 6,16	35,9 ± 4,9	<b>0,0001</b>
Conduit	11,10 ± 4,93	22,5 ± 4,2	<b>0,0001</b>
Booster	13,93 ± 7,37	13,4 ± 2,1	0,78

TS tako-tsubo syndrome; TTE transthoracic echocardiography; CMR cardiac magnetic resonance; RV right ventricle; LV left ventricle; EDV end-diastolic volume; ESV end-systolic volume; SV stroke volume; EF ejection fraction; BSA body surface area; E/A mitral valve E velocity divided by A-wave velocity; E/e mitral valve E velocity divided by mitral anular e velocity; PPT pulmonary transit time; PPTI pulmonary transit time index; PBVI pulmonary blood volume index.  
Mean +/- DS

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**Table 2: Univariable and multivariable logistic regression of CMR variables for discrimination TTC and control group.**

CMR variables	Univariable		Multivariable	
	OR (95%)	P-value	OR (95%)	P-value
PPT	0,38 (0.20-0.72)	0,003	0,57 (0.11- 2.72)	0,48
PPTI	0,41 (0.22 -0.74)	0,003	0.99 (0.32 – 3.16)	0,66
PBVI	0,98 (0.96 - 0.99)	0,009	1.01 (0.97 – 1.21)	0,03

PPT pulmonary transit time; PPTI pulmonary transit time index; PBVI pulmonary blood volume index.

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**Table 3: Correlation between Pulmonary transit parameters and echocardiography and CMR data in TS patients.**

	PBVI
<b>CMR parameters</b>	

EDV/BSA LV (mL/m <sup>2</sup> )	r= 0,330, p=0,133
ESV/BSA LV (mL/m <sup>2</sup> )	r=0,141, p=0,53
SV/BSA LV (mL/m <sup>2</sup> )	r=0,270, p=0,224
LVEF (%)	r=0,083, p=0,713
Left atrial area (cm <sup>2</sup> /m <sup>2</sup> )	r=0,220, p=0,310
Reservoir	<b>r=0,488, p= 0,021</b>
Reservoir strain rate	<b>r= 0,532, p=0,011</b>
Conduit	<b>r=0,498, p=0,018</b>
Conduit strain rate	<b>r=0,447, p=0,037</b>
Booster	r=0,262, p=0,23
Booster strain rate	<b>r=0,426, p= 0,048</b>
Global T2 mapping	<b>r= 0,520, p=0,019</b>
Global T1 mapping	r=0,180, p=0,473
<b>Echocardiography parameters</b>	
E/A	<b>r=0,443, p= 0,021</b>
E wave (cm/s)	<b>r=0,719, p= 0,001</b>
E/e	<b>r=0,683, p= 0,001</b>
<p>TS tako-tsubo syndrome; CMR cardiac magnetic resonance; LV left ventricle; EDV end-diastolic volume; ESV end-sistolic volume; SV stroke volume; EF ejection fraction; BSA body surface area; E/A mitral valve E velocity divided by A-wave velocity; E/e mitral valve E velocity divided by mitral anular e velocity; PPT pulmonary transit time; PPTI pulmonary transit time index; PBVI pulmonary blood volume index. Mean +/- DS</p>	

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